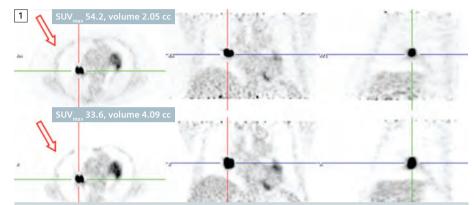
# Respiratory Motion No Challenge for HD•Chest

## Full HD Lesion Detection for Every Patient, Every Day

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The visualization and quantification of thoracic lesions by PET is complicated by respiratory motion, which often causes lesion blurring. This can lead to an overestimation of lesion volume, as well as under-estimation of radionuclide uptake by the lesion (expressed as the PET standardized uptake value or SUV). Motionrelated blurring is commonly seen in lung nodules, as well as in liver and pancreatic tumors. Lung tissue, especially in the lower lung, moves mainly in the superior-inferior direction. Respiratory motion can be as large as 3 cm for lesions in lung bases. One study (1) reported that the range of tumor motion varied from 8 mm to 25 mm among 5 lung cancer patients. In addition to the advancements in PET technology like improved spatial resolution, pointspread function techniques and Time of Flight, HD•Chest from Siemens has considerably improved the ability of small lesions to be visualized by eliminating the impact of motion related blurring on visualization and quantification. Conventional phase-based respiratory gating of PET acquisition decreases motion artifacts and partial volume effects and delivers accurate estimation of tumor motion and more precise measurement of the maximum SUV (SUVmax). However, traditional gated PET techniques are associated with considerably increased acquisition and post-processing time as well as high noise levels in individual gate images. Due to complex patient setup and the needed increase in acquisition time, conventional phasebased respiratory gating during PET acquisition has not yet become routine. Lower count levels in individual gates necessi-



This comparison of non-gated PET (bottom) and HD+Chest (top) in a large lung tumor at the hilar level shows significant increase in SUVmax and almost 50 percent reduction in tumor volume with HD+Chest due to elimination of motion related blurring. Such improved quantification especially of tumor volume has implications in radiation therapy planning and can potentially help decrease GTV in radiation planning similar to what has been demonstration by 4D gated PET. (Data courtesy of National Jewish Hospital, Denver, CO, USA)

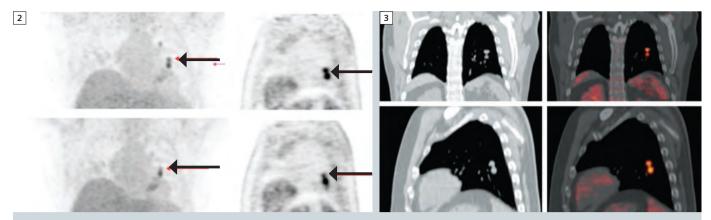
tate longer scan times in order to achieve adequate count statistics. A respiratorygated acquisition for a lung lesion in a single PET bed position my require 10 minutes, while standard non-gated PET images can be acquired in two to three minutes. In patients with irregular patterns of respiration, gated PET can lead to errors because of incorrect timing of data acquisition in the phase bins. Amplitudebased PET gating, which is a novel approach for gated PET acquisition, is a good method for respiratory motion reduction without the penalty of longer acquisition times and high image noise as seen in phase-based respiratory gating.

## Siemens Amplitude-Based Gating: HD•Chest

Siemens amplitude-based gating, HD•Chest, emphasizes that this approach delivers a high-definition PET image of the chest even though the patient breathes freely during the acquisition. HD•Chest integrates amplitude-based gating as an integral part of the whole-body PET acquisition and shortens the overall acquisition time compared to phase-based gating. This ensures images with minimum motion can be obtained for the relevant PET bed positions as part of the routine PET acquisition without undue increase in acquisition time as well as image noise as in 4D gated PET.

### **HD**•Chest—Initial Results

Early work using HD•Chest has been performed at the MAASTRO clinic in Maastricht, Netherlands. In 26 patients with lung tumors, non-gated PET, amplitude-based (HD•Chest) and 4D gated PET was compared. In general, SUVmax values calculated with HD•Chest and PET-4D were significantly higher than values calculated with non-gated PET. Average SUVmax values for 26 primary tumors were 12.9 ± 5.6



2 This case example shows improved separation of two malignant nodular lung lesions close to each other with HD•Chest (top) while blurring due to respiratory motion is apparent from the non-gated study (bottom) with poor visualization of the upper nodule.

3 Fusion of HD • Chest PET images with breathold CT in the same patient shows exact fusion of the two distinct hypermetabolic nodules with the nodules demonstrated on CT. Note the upper nodule is of similar size to the lower one. The upper nodule was however poorly visualized on nongated image due to respiratory motion related blurring. Data courtesy of University of Michigan, Ann Arbor, MI, USA.

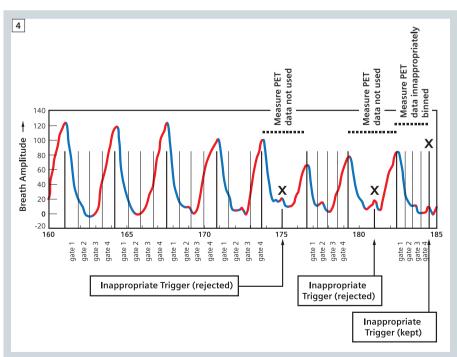
for non-gated PET,  $13.5 \pm 5.8$  for PET-4D, and 13.9 ± 6.7 for HD•Chest. SUVmax derived from HD•Chest was 6.6±9.1 percent higher than from non-gated PET but were similar to values generated by 4D gated PET. Calculation of SUVmax by PET-4D was associated with substantial variation between different gates. Intragate variation of SUVmax ranged from 2 percent to 13 percent, which demonstrates

the end of inspiration.

the potential for error in calculating SUV values from 4D gated studies. The authors concluded that HD•Chest provides a reproducible solution for accurate SUV calculation for tumors that move during the respiratory cycle.

Tumor volumes measured by HD•Chest and 4D gated PET were significantly less than tumor volumes measured with non-gated PET, probably because tumor

margins were less blurred by motion. However, calculated tumor volumes were similar between HD•Chest and averaged 4D gated PET. Visually, HD•Chest images were sharper than 4D gated PET images, with higher signal to noise ratios. Visual evaluation by radiologists confirmed that tumor margins were more easily visualized by HD•Chest than by non-gated PET, because there was less intrinsic motion blurring.



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#### Recommended Reading

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